Automated Non-invasive Video-Microscopy of Oyster Spat Heart Rate during Acute Temperature Change: Impact of Acclimation Temperature

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We developed an automated, non-invasive method to detect real-time cardiac contraction in post-larval (1.1–1.7 mm length), juvenile oysters (i.e., oyster spat) via a fiber-optic trans-illumination system. The system is housed within a temperature-controlled chamber and video microscopy imaging of the heart was coupled with video edge-detection to measure cardiac contraction, inter-beat interval, and heart rate (HR). We used the method to address the hypothesis that cool acclimation (10°C vs. 22°C—Ta10 or Ta22, respectively; each n = 8) would preserve cardiac phenotype (assessed via HR variability, HRV analysis and maintained cardiac activity) during acute temperature changes. The temperature ramp (TR) protocol comprised 2°C steps (10 min/experimental temperature, Texp) from 22°C to 10°C to 22°C. HR was related to Texp in both acclimation groups. Spat became asystolic at low temperatures, particularly Ta22 spat (Ta22: 8/8 vs. Ta10: 3/8 asystolic at Texp = 10°C). The rate of HR decrease during cooling was less in Ta10 vs. Ta22 spat when asystole was included in analysis (P = 0.026). Time-domain HRV was inversely related to temperature and elevated in Ta10 vs. Ta22 spat (P < 0.001), whereas a lack of defined peaks in spectral density precluded frequency-domain analysis. Application of the method during an acute cooling challenge revealed that cool temperature acclimation preserved active cardiac contraction in oyster spat and increased time-domain HRV responses, whereas warm acclimation enhanced asystole. These physiologic changes highlight the need for studies of mechanisms, and have translational potential for oyster aquaculture practices.

Keywords: oyster, oyster spat, video microscopy, acclimation temperature, heart rate, heart rate variability, aquaculture
INTRODUCTION

Cardiac control is relatively conserved between phyla, despite inter- and intra-species differences; for example, myogenic propagation of cardiac electrical impulses and the excitatory and inhibitory regulation of heart rate (HR) retain common design principles across evolutionarily distant organisms (Koester et al., 1979). Further, species in which cardiac control emerged prior to mammalian evolution, such as oysters, provide a means to examine the origins of physiologic and pharmacologic mechanisms of cardiac control. In addition to these mechanisms, filter-feeding oysters are part of a growing aquaculture or sustainable food futures industry, which is influenced by changing ocean environments due to development, pollution, and climate change (Doney, 2010; The WorldFish Center, 2011; Ruckelshaus et al., 2013). Thus, an understanding of the physiology and pathology of commercially-farmed species is increasingly important (e.g., aquaculture accounts for 90% of Tasmanian commercial fisheries production Skirtun et al., 2013 and 10,000 tons of oysters are produced annually in Canada2). The latter were designed to provide a feedback system, which precedes the use of “sentinel animals” coupled with biosensors (e.g., adult oysters and mussels) (Kramer and Foekema, 2001; Andrewartha et al., 2016) to monitor health in aquaculture environments.

Oyster spat reflect the early ontogeny of the physiology of cardiac control and represent a unique stage in the oyster life cycle, which is characterized by rapid growth not yet impacted by the energy-demanding process of spawning (Beiras et al., 1995). Commercially-farmed Pacific oysters are routinely housed in hatcheries during their larval and post-larval spat stages, where they are reared in carefully regulated conditions (e.g., consistent temperature, food availability) targeted for optimal growth. This differs from the natural environment of the Pacific oyster, or that of mature, farmed oysters. The transition from hatchery to inter-tidal farm challenges juvenile oysters and may alter growth; however, little is known about the impact of acclimation temperature (T\text{a}) on cardiac physiology or the adaptive mechanisms/responses available to oyster spat during acute environmental temperature changes.

Previous studies of HR in adult oysters and other bivalves or molluscs have relied on invasive imaging techniques that disrupt the integrity of one of the valves, a stressor that negatively impacts on results (Veitch, 1974; Koester et al., 1979). Limited non-invasive methods have been tested in mature invertebrates (Dieringer et al., 1978; Depledge et al., 1996; Curtis et al., 2000). Although innovative methods for zebrafish electrocardiogram (ECG) also rely on invasive approaches to assess cardiac rate (Liu et al., 2016), promising results have been reported for HR in Atlantic salmon alevins using microscopy (Polymeropoulos et al., 2014). We set out to develop a robust, automated method to non-invasively detect cardiac contraction for HR and heat rate variability (HRV) measurements in oyster spat maintained at different environmental temperatures (10°C vs. 22°C). Application of the method provides an assessment of the cardiac physiology of oyster spat during acute cold-temperature challenge, as well as illustrates the opportunity for KT to define the impact of environmental rearing practices on animal pathology. The latter could provide an early health assessment system, while controlling oyster chamber seawater flow and temperature (Figure 1). The system combined off-the-shelf components coupled with customized components employing the principles of Peltier elements (Peltier, 1834; Kubes et al., 1989; Correges et al., 1998). The latter were designed to provide a feedback control system between the chamber temperature and the Peltier element. In our protocols the system provided 2°C step changes in temperature in less than 80 s, although slower and more rapid changes are possible.

The system provided clear images of the contracting oyster heart (Figure 2 and Video 1). Contraction was routinely identified in real-time by the automated, commercial edge detection system, while non-detection (due to valve motion, feeding, waste clearance etc.) was easily identified by the experimenter for exclusion. Coupled with the data acquisition software, the edge detection system provided inter-beat interval (IBI; time between consecutive cardiac contractions) and HR for subsequent calculation of HRV responses of spat during acute temperature change. The system also provided visual (video) and quantitative means to assess the incidence of asystole (cessation of cardiac contraction). The oyster spat cardiac contraction detection system and its components (Figure 1) can be obtained and assembled by investigators with moderate effort to provide robust detection for the calculation of IBI and HR.

Apparatus and Software

The experimental set-up consisted of three components: an experimental chamber, a customized electronic temperature-controller, and video microscopy coupled with commercial edge-detection technology (Figure 1).

The experimental chamber was contained within a custom-fabricated 8 × 4.5 × 5 cm anodized aluminum block with a 2.5 cm-diameter bore drilled lengthwise through its center. At a depth of 2.5 cm into the bore (measured from upper block surface) a clear watch-glass was secured and sealed in place. Three

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small (∼1–1.5 mm diameter) ports were drilled into three of the block sides (depth of ca. 2 cm from upper block surface) to allow for the insertion of a thermocouple and seawater inflow/outflow tubes (catheter tubing inserted via permanently-affixed syringe tips).

Seawater was maintained at a depth of ca. 1 cm within the experimental chamber (bounded by the watch-glass and walls of the aluminum bore), with inflow and outflow rates of ∼2.5 mL/min (inflow: gravity drip; outflow: peristaltic pump and Pressure Servo Control; Living Systems Instrumentation, Burlington). The oyster spat, which were individually placed atop the watch-glass within the water, were trans-illuminated via a Microlight 150 fiber optic light source (Fibreoptic Lightguides Australia; AIS Optical) contained within the aluminum bore below the watch-glass chamber. A custom servo temperature controller maintained chamber water temperature within ±1°C of each desired experimental temperature (Texp) set-point by means of a heat sink (fan)-coupled Peltier element; feedback was obtained via the thermocouple inserted into the center port of experimental chamber.

The trans-illuminated oyster was visualized from above using a microscope (Zeiss Stemi SV6, Zeiss, Germany) coupled with a digital video camera (SONY Hyper HAD Color Video Camera, Japan). The camera video signal was transmitted in real-time to the computer via a video capture device (Roxio Video Capture – Roxio Central Fx/Roxio Central4; 60 fps) connected to edge detection hardware/software (V94 Video Dimension Analyzer, Living Systems Instrumentation, Burlington, Vermont). Edge detection was used to track cardiac motion in real-time by comparison of pixel color at a reference point in the video image (stationary area with no color change over time; see white line on right of Figure 2 and Video 1) with pixel color at an active area of interest (area of cardiac motion as indicated by significant color change over time; see left white line in Figure 2 and Video 1).

Analog edge-detection and thermocouple data were acquired for analysis via a data acquisition system (PowerLab 4/20, LabChart® 7 Pro; ADInstruments, Bella Vista, NSW, Australia). High-fidelity periods of detection were routinely obtained and used for analysis, while occasional segments in which edge detection was compromised were excluded from analysis (for example: short periods of active valve movement, excretion of waste). Detection of IBI (see Figure 2, square waveforms) was standardized to the leading edge of the raw edge detection.
waveforms, and analysis was performed using LabChart’s HRV software module with manual inspection of all analyzed data to confirm accurate detection. We adopted a working definition for cardiac asystole as fewer than 45 cardiac contractions within a particular 10 min protocol segment. This definition reflected the observation that periods of asystole presented as a series of increasingly slow, sporadic contractions at a cooler $T_{\text{exp}}$, after which complete asystole occurred and was sustained until a certain $T_{\text{exp}}$ was reached during the warming arm of the protocol.

**Model: Pacific Oyster Spat**
The juvenile spat stage follows the 15–30 day larval stage in the oyster life cycle, with few studies available compared with mature oysters (Albentosa et al., 1994; Beiras et al., 1995). During the spat stage oysters develop the morphology typical of bivalves, comprising a flat upper (right) valve and domed lower (left) valve joined at an anterior hinge by an adductor muscle. The spat is covered by two mantles, which participate in shell formation and sensation, and possesses two sets of gills, the vascular sites of gas exchange, in the mantle cavity (Quayle, 1969). As closure of the valves requires activation of the adductor muscle, bivalves preferentially keep their valves open unless faced with marked environmental changes, including acutely lowered temperature (Bernard, 1983). The myogenic oyster heart consists of two auricles and a ventricle, which supply a poorly-defined circulatory network that bathes tissues in blood that is returned to the heart via numerous veins; pulsating accessory hearts are also present, supplying circulation to the kidneys (Quayle, 1969). Oyster hearts are regulated extrinsically and intrinsically by neural, biochemical, and environmental/physical (e.g., temperature, pressure, salinity) mediators (Koester et al., 1979).

**Protocol**
Triploid *Crassostrea gigas* spat (age: 3.5–4 months, length: 1.1–1.7 mm) were obtained from a commercial hatchery (Shellfish Culture Ltd., TAS; hatchery temperature $\sim 22^\circ$C) and acclimated for a minimum of 2 weeks to either 10°C ($T_{a10}$, $n = 8$) or 22°C ($T_{a22}$, $n = 8$). Spat were maintained in aerated housing containers and supplied daily with hatchery-sourced, filtered seawater containing 2–3 million cells/mL of *Chaetoceros I* (TAS) and

**FIGURE 2 | Heart rate quantification.** Cardiac contraction detection was performed by a commercially available Video Dimension Analyzer (see text) that compared pixel color at an active point (tip of left white line, positioned above oyster; left panels) with pixel color at a reference point (tip of right white line, positioned external to oyster; left panels). The image directly surrounding the spat heart has been magnified to illustrate the color change of the heart at different points during the contractile cycle. The bottom left panel shows the location of the active point at its baseline value during relaxation of the heart. The top right panel shows how, based on gain, cardiac contraction and its resultant pixel color change caused deflection of the active point toward the reference point. The waveforms generated by the edge detector were acquired by the data acquisition system for subsequent analysis (right panel, bottom channel). The time between the leading edges of the onset of each contraction (green waveform detection dots; right panel) provided IBI and HR. Upper channel of the right panel is a record of water temperature as measured by the thermocouple during a period of temperature change between $T_{\text{exp}}$. See Video 1 for real-time edge detection imaging.
**Skeletonema pseudocostatum** (SA), then individually transferred into the experimental chamber (placement of right valve surface toward the video-camera unit).

The experiment consisted of a temperature ramp (TR) protocol, where the chamber was set to \( T_{\text{exp}} = 22^\circ C \) at the onset of the protocol, cooled to \( T_{\text{exp}} = 10^\circ C \) and re-warmed to \( T_{\text{exp}} = 22^\circ C \). This was done in 2°C intervals, with 10 min at each \( T_{\text{exp}} \) (Figure 3). The design of the chamber ensured oxygenation and food supply throughout the protocol (as above).

**Analysis**

Heart rate, Q10, and time- and frequency-domain HRV analyses were calculated for the data using Excel. During the TR protocol we noted that the spat routinely displayed asystole as a component of the physiologic response to cool \( T_{\text{exp}} \) and, therefore, quantified the occurrence of asystole for each acclimation temperature (\( T_a \)) group.

Preliminary HRV analysis was applied in the time and frequency domains using scaling factors similar to human HRV, since spat HR was similar to human values. As a result, the scaled time-domain analysis parameter, pNN50, was used across the tested \( T_{\text{exp}} \). The four time-domain parameters studied were: mean IBI, SDNN (standard deviation of normal IBIs), RMSSD (the root mean square of successive differences of successive IBIs), and pNN50 (the percentage of normal IBIs differing from their preceding IBI by more than 50 ms). Only oysters with active cardiac contraction (i.e., not in asystole) were considered in HRV analyses.

Frequency-domain HRV analysis of IBIs was performed using Kubios software (Kubios HRV version 2.1, University of Eastern Finland, Kuopio, Finland; Tarvainen et al., 2014). Our analysis revealed that oyster spat power spectra failed to display clear peaks aligned with the low- and high-frequency domain peaks used to justify frequency domain analysis in mammalian species (Thireau et al., 2008). As a result, we restricted our HRV analyses to the time domain.

Statistical analyses were performed using SAS V9.4 (SAS Institute Inc., Cary, NC, USA). In order to assess the acute cardiac response to temperature change and the impact of \( T_a \), which reflects the transition from hatchery to open aquaculture environment, we compared rates of asystole within acclimation groups. Rates of asystole were compared between \( T_{\text{exp}} = 10^\circ C \) and \( T_{\text{exp}} = 22^\circ C \) by McNemar’s exact test. The difference in asystole rates at 10°C between acclimation groups was tested by Fisher’s exact test. Continuous outcomes (HR and HRV parameters) were modeled by the linear mixed effect model estimated by restricted maximum likelihood as implemented by the MIXED procedure of SAS V9.4. The model included fixed effects for acclimation group, temperature, phase (warming vs. cooling), and an acclimation group by temperature interaction to allow comparison of temperature slopes between acclimation groups. The model accounted for the repeated serial measures on spat by including a random effect for spat and allowing for within-spat first order auto-correlated residuals. Q10 values between and within groups were assessed via 2-way ANOVA on ranked data with Shapiro-Wilk and Brown-Forsythe tests. Mean values were reported as mean ± SEM. SEM was not presented in cases where, due to asystole, \( n < 4 \) for a given group. All tests were two-sided without correction for multiplicity.

**RESULTS**

**Cooling-Induced Cardiac Asystole**

Oyster spat routinely adopted cardiac asystole during cooling, and the occurrence of asystole was inversely related to \( T_{\text{exp}} \) (Figure 4). During cooling from 22°C to 10°C the percentage of spat in asystole increased from 0 to 100% in the \( T_{a10} \) group (\( P = 0.008 \)) and from 0 to 38% (\( P = 0.25 \)) in the \( T_{a22} \) group. The 62% difference in asystole at 10°C was statistically significant (\( P = 0.026 \)). Figure 4 shows that cardiac activity ceased at higher \( T_{\text{exp}} \) during the cooling phase than the \( T_{\text{exp}} \) at which it resumed during warming in \( T_{a22} \) spat.

**Spat Heart Rate Responses**

Mean spat HR was positively associated with \( T_{\text{exp}} \) in both acclimation groups (Figures 5, 6). In \( T_{a22} \) spat the average initial HR at 22°C was 83.2 beats/min (95% CI, 70.8–95.7) and this decreased by an average of 7.3 beats/min (5.9–8.7, \( P < 0.001 \)) per degree Celsius during cooling (when asystolic spat, as defined in Methods and Materials, were included in calculations as HR = 0). In \( T_{a10} \) spat the mean initial HR at 22°C was 78.6 beats/min (66.2–91.1) and this decreased by an average of 5.1 beats/min (3.7–6.5, \( P < 0.001 \)) per degree Celsius during cooling (including asystolic spat as HR = 0). The HR of \( T_{a10} \) spat at the initial 22°C acute temperature was not different from the \( T_{a22} \) spat (difference in HR between \( T_{a10} \) and \( T_{a22} \) = 4.6; −11.7 to 20.9; \( P = 0.57 \)), however, they did exhibit a lower rate of decrease during cooling (difference = 2.2; 0.3–4.2; \( P = 0.026 \); this included asystolic spat as HR = 0). Excluding spat in asystole, the average decrease in heart rate per degree Celsius while cooling was 5.5 beats/min (4.6–6.3, \( P < 0.001 \)) within \( T_{a22} \) compared to 4.3 beats/min (3.7–4.9, \( P < 0.001 \)) within \( T_{a10} \) with a significant difference in slopes between acclimation groups (being 1.1; 0.1–2.2, \( P = 0.032 \)).

Figure 5 shows that in the \( T_{a10} \) group the \( T_{\text{exp}} \) specific HR was similar during cooling and warming regardless of inclusion of asystolic spat. However, in the \( T_{a22} \) group, the HR appears to have dropped more quickly during cooling due to the increased proportion of spat in asystole. The cooling and warming patterns in \( T_{a22} \) spat did not vary substantially when restricting analysis to spat that maintained active cardiac contraction (i.e., excluding...
FIGURE 4 | Prevalence of asystole during temperature ramp protocol. Proportion of oysters in asystole or maintaining active cardiac contraction (n=8) expressed as a percentage. Left Panel: Percentage of spat maintaining active cardiac contraction at each T_{exp}. Circles/gray bars represent T_{a10} spat; squares/black bars represent T_{a22} spat. Right Panel: Percentage of spat displaying asystole at each T_{exp} (<45 beats/10 min). Both Panels: Asystole occurred at low T_{exp}. The percentage of spat in asystole was greater at 10\degree than 22\degree in T_{a22} spat (P = 0.008; horizontal gray bar ***), and there was a 62% difference in the prevalence of asystole between T_{a22} and T_{a10} spat at 10\degree (P = 0.026; vertical dashed line *).

FIGURE 5 | Effect of temperature (Cooling vs. Warming) on heart rate profile. HR was directly related to T_{exp} in both acclimation groups independent of asystole. Left panels: Mean HR ± SEM of spat showing active cardiac contraction (asystolic spat excluded). In T_{a22} spat, HR decreased at an average rate of 5.5 beats/min per degree Celsius during cooling when asystole was excluded, whereas in T_{a10} spat it decreased by an average of 4.3 beats/min per degree Celsius during cooling when asystole was excluded (both P < 0.001; horizontal line ***). T_{a10} spat displayed a lower rate of HR decrease during cooling than T_{a22} spat (P = 0.032). Right panels: Mean HR ± SEM of all spat (asystolic spat included). In T_{a22} spat, HR decreased at an average rate of 7.3 beats/min per degree Celsius during cooling when asystole was included, whereas in T_{a10} spat it decreased by an average of 5.1 beats/min per degree Celsius during cooling when asystole was included (both P < 0.001; horizontal line **). T_{a10} spat displayed a lower rate of HR decrease during cooling than T_{a22} spat (P = 0.026).
asystolic spat from analysis). **Figure 6** (left panel) shows that among spat with active cardiac contraction, $T_{a22}$ and $T_{a10}$ had a similar HR response to $T_{\text{exp}}$.

**Impact of Acclimation on Q10**

Q10 values for mean HR were calculated in the cooling and warming phases for spat in each acclimation group (mean ± SEM). There were no significant differences in Q10 between $T_a$ groups, between the warming vs. cooling phases within $T_a$ groups, or interactions between $T_a$ and phase (Q10 values: $T_{a22}$ – cooling phase: $2.6 ± 0.3$, warming phase: $2.4 ± 0.2$; $T_{a10}$ – cooling phase: $2.4 ± 0.2$, warming phase: $2.7 ± 0.3$; all $P > 0.05$, 2-way ANOVA).

**Impact of Acclimation on HRV**

There was an inverse relationship between each of IBI, RMSSD, SDNN, and pNN50 with $T_{\text{exp}}$ in each acclimation group (after excluding spat in asystole, all $P < 0.01$ for association with $T_{\text{exp}}$; **Figure 7**). At any given $T_{\text{exp}}$, RMSSD and pNN50 were significantly higher in the $T_{a10}$ group than the $T_{a22}$ group (both $P < 0.001$), but there were no differences between $T_{a10}$ and $T_{a22}$ groups for IBI ($P = 0.11$) or SDNN ($P = 0.13$; both **Figure 7**).

**DISCUSSION**

We developed an automated, non-invasive, real-time method to detect cardiac contraction and measure HR and HRV in trans-illuminated triploid Pacific oyster spat (*Crassostrea gigas*). The system used video microscopy, edge-detection technology, and a custom-built experimental chamber. We applied the method to assess cardiac responses to acute temperature changes on a background of cool or warm environmental acclimation temperatures. The results suggest that spat may be a promising novel model species to explore conserved mechanisms of HR control. Our method and the results of its first application also have KT implications, since they can be used to assess hatchery practices that influence growth rates, survival, or the physiology of oyster spat prior to placement in the open aquaculture environment (Newell and Branch, 1980; Bernard, 1983; Helm, 2005). The acclimation temperatures of $10^\circ$C ($T_{a10}$) and $22^\circ$C ($T_{a22}$) reflect aquaculture industry practices, i.e., hatchery temperature ($22^\circ$C) and a cool temperature that may be encountered upon introduction to an open, temperate aquaculture environment ($10^\circ$C). We provide the first measurements of the prevalence of asystole, HR response, and time-domain HRV profile of spat exposed to an acute temperature ramp (TR) protocol from $22^\circ$C to $10^\circ$C to $22^\circ$C. Cool temperature acclimation lowered the incidence of asystole in $T_{a10}$ acclimated spat vs. $T_{a22}$ spat and was accompanied by greater HRV. The presence of asystole suggests that oysters reared in the normal hatchery environment ($22^\circ$C) may be negatively impacted as they are placed into open ocean environments.

**An Automated, Non-invasive Solution to Measure Juvenile Bivalve/Small Invertebrate Heart Rate**

Our system takes advantage of the relatively stationary nature of bivalves and the translucence of spat shells. The experimental chamber enabled rapid changes in $T_{\text{exp}}$ during which cardiac contraction and HR could be assessed relative to $T_a$. The system can provide rapid as well as slow temperature changes, which contrasts with existing reports, where experimental chambers are placed or immersed within large, temperature-controlled water baths to make cardiorespiratory or metabolic measurements (Frappell and Mortola, 2000; Polymetrooulos et al., 2014).

Adult oyster hearts have previously been studied *in vitro* and *in vivo* (Greenberg, 1965; Greenberg et al., 1980; Andrewartha et al., 2016), largely through invasive means that disrupt valve integrity to view/record from the exposed heart and negatively influence outcomes (Vetch, 1974; Koester et al., 1979). For example, HR has been measured by incident
laser beam reflection from the heart through a several mm diameter hole (Ritto et al., 2001, 2003; Hellicar et al., 2014). Ultrasound stethoscopes (Dieringer et al., 1978) or infrared diodes/phototransistor detectors (Depledge and Andersen, 1990; Depledge et al., 1996; Curtis et al., 2000) have been reported to measure bivalve HR non-invasively. However, the large hardware components make this incompatible with spat (<2 mm) and these approaches have limited means for verifying that only HR is being detected. By contrast, the thin valves of young spat are amenable to trans-illumination, eliminating physical stressors and attachments, while video microscopy provides an easily verifiable HR signal for the experimenter. Our automated, non-invasive method could be applied to younger or older spat once the limits of microscopic magnification and shell calcification (i.e., animal maturity and size) are defined, or in other species amenable to trans-illumination (e.g., other invertebrates, alevis, Polyméropoulos et al., 2014; eggs, Mortola et al., 2010, 2012). We used the minimum light intensity necessary for cardiac visualization; however, near red light sources could be used to determine/minimize the potential impact of light exposure on spat physiology. The system could also be adapted for use “in the field” in open, aquaculture environments.

Methodology Application: Pacific Oyster Spat Cardiac Responses to Environmental Temperature Change

Oyster growth is most rapid at warm temperatures with high food and oxygen availability (Walne and Spencer, 1974); however, the cardiac control phenotype during temperature challenge was not known. As cultured oysters are initially reared in hatcheries providing constant, ideal conditions, our data on the impact of acute changes in variables such as $T_{\text{exp}}$, such as those encountered upon initial ocean exposure, suggest ways to measure/improve species health and production.

Cool Temperature Acclimation Decreases Asystole Occurrence at Low Temperatures

The asystole induced during cooling was inversely related to $T_{\text{exp}}$, and was more prevalent in $T_{222}$ spat ($8/8$ asystolic at $T_{\text{exp}} = 10^\circ \text{C}$; Figure 4). Residual beats were generally observed at the onset of a cooler $T_{\text{exp}}$, after which complete asystole occurred and was sustained until $T_{\text{exp}}$ increased during the warming arm of the TR protocol. This is consistent with a report for the adult blue mussel ($Mytilus edulis$), where asystole occurred at $<8^\circ \text{C}$ if $T_a = 18^\circ \text{C}$.
Cool Temperature Acclimation Increases Heart Rate Variability

Time- and frequency-domain HRV analyses are used to investigate autonomic cardiovascular control (ESC/NASPE Task Force, 1996; Tarkiainen et al., 2005; Thireau et al., 2008). Myogenic molluscan hearts have diffuse pacemaker properties, receive modulatory input from extrinsic cardiac nerves, and are regulated by a combination of neural, biochemical, and environmental/physical (e.g., temperature, pressure, salinity...) mediators (Divaris and Krijgsman, 1953; Trueman and Lowe, 1971; Trueman et al., 1973; Lowe, 1974; Irisawa, 1978; Koester et al., 1979; Ritto et al., 2005). HRV analysis assumes that beat-to-beat variations in HR (i.e., inter-beat intervals, IBIs) are effected by neural modulation (Sandercock and Brodie, 2006; Chattiapakorn et al., 2007; Domnik et al., 2012). There is debate on whether to correct for non-cardiac physiologic rhythms (e.g., respiratory sinus arrhythmia) when performing mammalian HRV analyses; however, many studies employ raw HR in the calculation of HRV (Tzeng et al., 2003; Thireau et al., 2008). HRV application to invertebrates is rare, and the relative neural, physical and/or hormonal modulation of HR in oysters has not been fully elucidated (Greenberg, 1965; Quayle, 1969; Mayeri et al., 1974; Liebeswar et al., 1975; Hill and Yantorno, 1979; Koester et al., 1979; Greenberg et al., 1980). Thus, we adopted an approach that performed HRV calculations based on raw HR data, analogous to that employed in mammals.

Few studies have explored HRV in bivalves (Curtis et al., 2000; Ritto et al., 2005). Our analyses revealed none of the defined spikes in post-spectral density (PSD) at specific frequencies as seen in mammals, which is an interesting biologic observation that precluded the application of frequency domain HRV analysis (ESC/NASPE Task Force, 1996; Curtis, 1998; Curtis et al., 2000; Thireau et al., 2008). Mussels have also been reported to have no spikes in PSD (Curtis, 1998; Curtis et al., 2000). The hypothesis of independent control of HR, distinct from ventilation or other physiological functions, is one that deserves further attention. Time-domain HRV analysis (IBI; SDNN; RMSSD; pNN50) applied to oysters not in asystole revealed that all HRV variables were inversely related to \( T_{exp} \) (Figure 7). This is similar to findings in mammals, where HRV is inversely related to HR (Billman, 2013; Sacha et al., 2013a,b). It is also reminiscent of the response reported for toxin exposure (e.g., copper), where an inverse relationship between coefficient of variation (variability) and HR was present in mussels (Curtis et al., 2000). Both acclimation groups had low HRV at \( T_{exp} \) of 22°C, consistent with low HRV in mussels at control conditions (Depledge et al., 1996; Curtis et al., 2000). This varies from the marked HRV in resting mammals (ESC/NASPE Task Force, 1996; Thireau et al., 2008; Domnik et al., 2012), and may reflect a greater scope for beat-to-beat neural regulation of HR in mammals. \( T_{a10} \) spat had increased HRV compared to the \( T_{a22} \) group (RMSSD and pNN50).

Our findings raise the question of how best to compare and interpret HRV in invertebrates and mammals. Baseline HRV differs between invertebrates and mammals; however, the inverse relationship between HR and HRV remains (Depledge et al., 1996; Kazuma et al., 1997; Curtis et al., 2000; Gong et al., 2004). In mammals, HRV reflects overall autonomic balance and decreased HRV is a negative prognostic indicator (Sandercock and Brodie, 2006; Chattiapakorn et al., 2007); one possible interpretation of our findings is that increasing HR at decreased \( T_{exp} \) may suggest the inverse for invertebrate species. We speculate that the adaptive thermal compensatory response to cold \( T_{exp} \) and \( T_a \) may increase HR in aquatic invertebrates, similar to copper (Curtis et al., 2000) or starvation (Depledge et al., 1996). Further work is required to elucidate the details of this relationship, since \( T_{a10} \) spat were less likely to become asystolic at cool
temperatures despite exhibiting higher HRV than T \textsubscript{a22} spat with active HR. The potential predictive power of HRV could be tested using the impact of known stressors (including low food availability and Pacific Oyster Mortality Syndrome (POMS)), which negatively impact on the physiology, growth, and viability of oysters (Widdows, 1973; Duthie, 2014; Andrewartha et al., 2016). The impact of environment on oyster outcomes has been approached through the development and application of habitat suitability indices (HSI); however, outcome measures typically rely on mortality/viability as the primary outcome (Brown and Hartwick, 1988; Theuerkauf and Lipcius, 2016). Evaluation of oyster HR or HRV is the physiologic complement to HSI assessments and has the potential to provide insight into animal health prior to overall mortality measures, as well as to allow the detection of acute environmental changes. Indeed a recent report in the adult oyster suggests that biosensors could monitor HR and health in “sentinel” animals (Andrewartha et al., 2016). This concept is similar to those proposed for other species, such as zebrafish, as biological models or pharmacologic screens (Liu et al., 2016; Rahbar et al., 2016). HRV has been used to explore cardiac regulatory mechanisms, which could be employed to assess cardiac phenotype between triploid and diploid spat or other marine invertebrates. Acclimating oyster spat to lower temperatures prior to release in ocean oyster beds may enhance adaptability to temperature-variable environments, and provide the means to test for early signs of adaptive or compensatory responses to negative environmental changes.

CONCLUSIONS

We developed an automated, non-invasive video-microscopy system to detect cardiac contraction for the real-time measurement of IBI, HR, and HRV in oyster spat that were maintained at different environmental temperatures. The impact of temperature challenge on oyster spat HR and HRV suggests that spat provide a model for conserved mechanisms of cardiac physiology, and also illustrates the potential for knowledge translation to the aquaculture industry. Cooling more readily induced asystole in warm-acclimated spat, although the molecular mechanisms responsible for the ontogeny of the cardiac asystole response remain to be elucidated. Indeed, the energetic cost of such a response may vary at different points in the oyster life cycle, reflecting the strength of the underlying link between cardiac and metabolic control. Our time domain HRV data, the first from oyster spat, require further investigation to determine whether the directionality of HRV changes induced by deteriorating health in mammals is conserved in invertebrate species. Our data suggest that optimization strategies for hatchery temperatures could impact growth/survival in the transition to ocean farms. The method provides a new tool to assess spat resilience to environmental changes or strategies to minimize early spat mortality in open waters (Mann, 1979). Incorporation of measurements of metabolic rate, filtration rate, or growth would provide an integrated analysis of the energetic cost of the observed HR alterations in variably-acclimated spat.

AUTHOR CONTRIBUTIONS

ND: Design of experiments/hypotheses; methodologic design; performed experiments; analysis/interpretation; wrote and revised manuscript. EP: Assisted with experiments, experimental/methodologic design, interpretation; editing of manuscript. NE: Assisted with experiments, experimental/methodologic design; editing of manuscript. PF: Design of experiments/hypotheses; methodologic design; interpretation; editing of manuscript. JF: Design of experiments/hypotheses; methodologic design; assisted with experiments; interpretation; writing/editing of manuscript.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: http://journal.frontiersin.org/article/10.3389/fphys.2016.00236

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